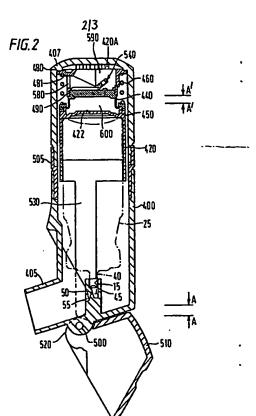
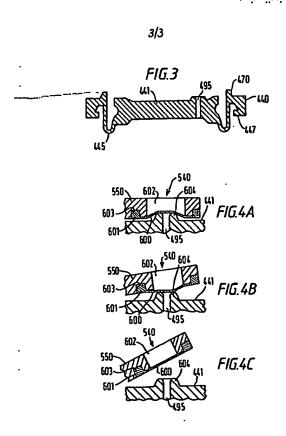


1/3

14 +0 90





\*5 35

## HEDICAMENT DISPENSING DEVICE

This invention relates to a dispensing device, and nore specifically, to a device suitable for dispensing discrete encounts of fluid or particulate naterial entrained in an air flow. The invention is concerned particularly, but no enclusively, with a dispensing device of the type where the natured dose is administered in response to the inhalation of the patient.

Hotered dose inhalers are well known in medicine for treatment, or alleviation of the effects of respiratory compleints, for example asthma. Breath-actuated devices are also known, and have been the subject of many patent amplications.

GB 1208971; GB 1297993; GB 1335378; GB 1383761; GB 1392192; GB 1413285; WO 85/01880; GB 2204799; GB 4803978 and EP 0186280A describe inhalation-actuated dispensing devices for use with a pressurized earosol dispensing container. The device includes a dispensing container and the container includes a valve capable of releasing a netered amount of the aerosol contents, when an internal spring operating the valve is compressed by a sufficient amount. The dispensing device often comprises a chamber having a mouthpiece, air inlets, actuating means for causing the actuation of the valve in the dispensing container, a latching means for releasably retaining said setaring valve in a charged position, and an inhalation responsive means for releasing the latch, such that a metered amount of serusol compound is discharged into the region of the mouthpiecs. The overall objective is to give coordination of discharge of medicament from the merosol container with inhalation of the potient, thus allowing a maximum dose of medicament to reach the brunchial passages of the lungs.

The invention provides a dispensing device for use with a drug delivery system, the dispensing device comprising means for releasing a dose of medicament from the system, the ....releasing means comprising means for applying a preload capable of actuating the drug delivery system to dispense a dose of medicament, means for applying a resisting pr or other gas force expable of preventing actuation of the drug delivery system, and a release device capable of freeing the resisting pneumatic force to allow the prelond to actuate the delivery means and dispense the medicament, wherein said resisting pnecesatic force is provided by a volume of gas held at a positive or negative pressure with respect to embient pressure, and said release means comprise a flexible plete-like sealing element which seals with a valve seat around a valve port, the opening of which releases said positive or negative pressure, the sealing element being carried by a sealing number such that, on initial movement of the scaling number, the scaling element flower as it is held by said positive or negative pressure against the valve seat until it is finally removed therefrom on further powement of the scaling nember.

Such a construction provides a more effective opening of the valve port giving a more consistent and a faster actuation of the valve.

The release device may be adapted to remove said scaling element from the valve seat in response to inhalation at an outlet mousle of the device.

The scaling element may be a disphrage scaling element held by the scaling number at its pariphery to provide a freely flexible central part which cooperates with the walve scat.

Although this device has been described in particular relation to a system using air, it will be realised that in a closed system any suitable gas could be used.

A device according to the invention is particularly suited for use with pressurized inhalation percepts having valves which can be actuated to dispense a dose of medicanent. The latching means is often commerced to a valve which moves from a latching position to a dispensing position in response to a partial vacuum developed upon inhalation.

EP-A-0045419 describes an inhalation device having biassing means which are alone of insufficient force to .... degrees the container but which together are of sufficient force to do so.

EP-A-186280 describes a device which employs magnets to control the release of the serosol container.

US 3605738 describes devices in which the aerosol container communicates with the nouthplece via a netaring channer. A netered quantity of the aerosol compound is discharged into the netering channer and this is conveyed to the nouthplece via an inhalation-actuated valve.

GB 1269554 describes a device wherein the sercool container is novable by a lever and can system into a charged position held by a latch, a pressure differential acting to trip the latch and nove the valve of the container to a discharge position.

International application So. PCF/GD91/02118 describes a netered dose inheler in which an axially movable dose dispensing assembly is subjected to a preload capable of actuating the delivery means thereof. This preload is itself subjected to a resisting passmatic force capable of preventing such actuation. A breath-actuated release valve is provided which, upon actuation, releases the resisting force to allow the preload to actuate the dose dispensing assembly. A pensuatic chamber is utilized for providing the resisting pneumatic force which may be a positive pressure, above atmospheric. A breath actuated release valve opens a valve port in said pneumatic chamber to release the resisting pneumatic pressure existing therein.

It is an object of this invention to provide an inhalar, preferably a breath actuated inhalar, having an improved release valve for releasing the resisting gas pressure existing in the aforesaid chamber.

However in other embodiments, a device according to the invention can be used with a dry powder drug delivery system disposed within a bousing of the device, in which a dose of powdered medicasent is dispensed by said system into an air flow in said housing created by inhalation at an outlet nossle of the housing.

In some arrangements according to the invention for use with an aerosol dispensing centainer, the housing may include an inner sleeve for enclosing the main body of the aerosol container to define a chanber for the aerosol container. The chanber may be defined at one end by a cross member which accommodates the valve of the aerosol and seals the chanber apart from providing an aerosol outlet. The inner-sleeve in preferably sealed such that there is sliding sirtight contact with the sleeve chanber such that the serosol container and inner sleeve provide a piston effect against the cross member to form the resisting load in the form of a high pressure volume capable of preventing the actuation of the aerosol valve.

In other arrangments according to the invention for use with an aerosol dispensing container, the housing may include an immer sleeve for enclosing the top portion of the sain body of the serosol container. This inner sleeve is preferably arranged to form one end of an airtight piston cylinder, bellows or disphragm, such that novement of the immer sleeve will result in an increase in the enclosed volume within the piston cylinder, bellows or disphragm producing a vacuum or low pressure volume to form the resisting load (force) capable of preventing the actuation of the serosol valve.

In some embodiments, the sleeve for the dispenser may act as a sliding, airtight piston, except that instead of providing a high pressure volume, downwards motion away from the main casing creates a low pressure volume.

In a preferred arrangement, the pmemmatic resisting means is formed by the inner sleave and a fixed insert in the outer chamber linked together by flexible bellows or by a sliding airtight seal between the slesve and a cylindar-like extension to the insert.

According to a feature of the invention, the preload may be provided by a spring which operates, for example, egainst the sarozol valve. Preferably the preload is applied by a lever, pivoted in a recess housed in the outer chamber. The lever may take the form of a restraining lever preventing a loaded spring from acting on the serosol can until operated. Arter operation the lever is used to reload the spring. Alternatively the lever may be connected via a plug to a spring which is in contact with the inner elseve such that movement of the lever loads the spring.

The release beans may comprise said valve port provided in the aforesaid cross number. The valve port may normally be covered by said flexible disphrage sealing aleasent which on actuation is opened, allowing the preload to actuate the sarusol valve as pressure in the present cannot return to the rest state. In the embodiment wherein the resisting force is a positive pressure of air, opening of the valve port releases the built-up pressure, and air escapes from the enclosed volume, allowing the full force of the preload to act against the aerosol valve. In the embodiment wherein the resisting force is a vacuum or near vacuum, opening of the valve port allows air to enter the enclosed volume, again allowing the full force of the preload to act against the aerosol valve.

A preferred breath-octuating release means comprises a novable vane mechanism. This vane mechanism may be housed in the lower or upper part of the chamber, depending upon the location of the resisting element. Said flexible disphrage sealing element is preferably strached to said vane, such that on inhalation the vane moves from its rest position closing said inlet means to its actuating position, thus moving the sealing element out of contact with the valve port, causing the opening of the valve. The vane mechanism is preferably dynamically balanced, and may be biassed towards its closed position, e.g., by a spring.

The opposite end of the dispensing container is contained within a sleave 420 of similar cross section to the main body 400. The longitudinal exis of both the sleave 420 and main body 400 is generally coaxisl. The sleave is in loose sliding contact with the inner wall of the main body to ellow free passage of air in the main body past the sleave. The sleave 420 may be held in place by commention with a disphrage 440 held in connection with the top of the main body 400, ms will now be described. Thus, the sleave 420 affectively hange from the top of the main body.

One end of an e.g., noulded flexible disphrage 440 (as shown alone in Figure 3) comprising a rigid disc-like section 441, a flexible generally cylindrical wall section 445 and-a stiffer connector section 447, is fitted around a purpose-unde groove 450 in the sleeve, e.g. by enap-fitting. A further noulded lip 470 on the disphrage provides a smng fit for one end of a compression spring 460. The compression spring is thus located and free to act on the sleeve. The other end of the compression spring is located by an annular shoulder 481 in a predominantly cylindrical flanged insert 460 housed in the top section of the main body 400. This insert includes a groove 490 into which the disc-like section 441 of the flexible disphrage 400 is snap-fitted.

The joint between the disphragm connector section 447 and inner sleave groove 450 is arranged to be airtight and the shape of the top surface of the cleave 422 to conform to the internal shape of the disphragm such that in the rest position of the inhalar the two surfaces are in close proximity, and the enclosed space between them very small.

The cylindrical insert 480 is retained in place by the end cap 407 of the main hody of the device. This forms a chamber 590 between the sir inlet slots 420 and the rigid part 441 of the disphrage. The chamber is provided with one or more air pathways 580 such that air may pass from the sir inlet slots 430 to the mouthpiece 405. As best seen in filed, the rigid disc-like section 441 of the disphrage also includes a small valve port 455 which is normally covered by

Air inlets may take the form of slots in the wall of said housing.

The medicament may be a drug per se or on any form of Carrier, e.g., including a powder or a gaseous carrier. The invention will now be described by way of example

only, with reference to the accompanying drawings, in which:

Pigure 1 is a sectional view of an inhaler embodying the
invention;

Figure 2 is a sectional view of the inhaler of Figure 1 with its nouthpiece dust cap in an open position;

Figure 3 is an enlarged view of a disphraga used in the inhaler shown in Figures 1 and 2; and

Figures 4A - 4C are respective diagrammatic illustrations of the release valve incorporated in the inhalar of Figs. 1 and 2, shown in three positions thereof.

Enfarring to the drawings, there is shown an inhalation device which is essentially similar in construction and operation to the device described in International Patent Application So. PCF/GB91/03118 (the disclosure of which is incorporated harain by reference) with reference to Figures 3 to 5 thereof. The modification thereof according to the present invention will be described below.

The inhelation device consists of a main body or housing 400 which is generally cylindrical in cross section, with a mouthpiece section 405 at one and and an end cap 407 housing air inlets 420 at the other end. A known type of acrosol dispensing container 25 of generally cylindrical shape is boused within the nain body of the device. The acrosol dispensing container has a stem 40 which contains an acrosol dispensing valve (not shown). The bore 15 is such that it forms an airtight seal on the stem 40 of the acrosol dispensing container 25. A shoulder 45 limits and locates the position of the stem 40, which in turn locates the acrosol dispensing container 25 in position in the main body 400. A passage 50 artends from the bore 15, continuing from the shoulder 45 to interconnect with a dispensing nozale 55.

a valve seal 540 housed in a vane 550 pivotally connected to the insert 480. The vane 550 may be bisseed closed by a light spring flamure, a weight or a magnet (not shown).

The valve seal 540 is in the form of a flexible elastemeric disphrege scaling element 600 having an annular ris 601. The scaling element 600 is drawn over an eperture 602 in the vane 550 whereby the central part the scaling element 600 is freely flexible. The annular ris 601 is located in an annular grove 601 provided in the vane 550 around the lower and of the aperture 602.

The vane 550 in its rest position divides the chasher 590 between the sir inlets 420 and the sir pathways 550 that link to the nouthpiece such that it may nove from its rest position by means of a pressure drop between the sir inlets and the mouthpiece. On novement of the vane to the actuated position the sealing element 540 is sufficiently noved to open the value nort 495.

The elastomeric disphragm sealing element 600, in the closed position of the valve as shown in Figure 4A, is drawn tightly ower a raised annular seat 604 provided around the valve port 495. This arrangement provides a very compliant seal, which can easily accommodate variations in alignment caused by an accumulation of tolerances and also requires only a very light return spring on the vane 550 to ensure the seal is re-made. Moreover, as the flap starts to open as shown in Figure 4B, the sealing element 600 will be retained in sealing engagement with the valve seat 604 by vacuum pressure, until the seal is smidenly and completely invites, as shown in Figure 4C, allowing the vane to drop complete (Figure 2) thereby fully opening the valve port 495 and thus ensuring commistant and fast actuation of the valve.

Other sealing arrangements could allow air to leak through the valve port, if the valve opens slowly which could lead to an inconsistent actuation of the device.

As shown in Figures 1 and 2, the end of the main body having a pivot 500, has a recess sdapted to receive a can 520 integral with a dust cap 510 operating on the pivot. The recess further includes a passage communicating with a similar passage moulded into the internal wall of the main body 400. A can follower in the form of a yoke 530 secured to the lower edge of the inner sleeve 420 acts on the cas such that when the dust cap is in the closed position the inner eleave is forced by the can follower to its uppermost position.

When the dust cap is rotated to its open position the cam profile is such that the cam follower is free to nove downwards by an amount sufficient to allow actuation of the dayles.

In its rest position with the dust cap 510 closed, the cam follower 530 restrains the inner sleeve 420 in its uppermost position such that the enclosed space trapped between the disphraga 440 and the top surface 422 of the inner sleeve is at a minimum and the spring 460 is compressed. The valve port 495 is closed by the valve scal elegant 540 and the sleeve 430 is clear of the top of the serosol can 25 which is then unleaded.

The dust cap is opened rotating the integral can 520 allowing the can follower 510 to drop by amount AA. The inner slesve is forced downwards under the action of the spring 460. As the inner slesve noves downwards the enclosed volume between the disphram 440 and inner slesve is increased by a linear equivalent amount A'A', less than or equal to AA. Since the valve port 495 is closed this creates a low pressure volume or near vacuum in the space 600. The effect of the pressure differential between the enclosed volume 600 and atmospheric pressure is such that the inner slesve tends to resist the action of the spring. As the inner slesve moves downwards it contacts the sacrosol can 25 and begins compression of the serosol valve (not shown).

powward movement of the inner sleeve will continue until there is a belence of forces between the compressive force in the spring 460 and resisting forces created by the pressure differential and compression of the aerosol valve. The geometry of the device is arranged such that this belance

11

seal element is only lightly biassed to its closed position it presents little resistance to air flow out of the enclosed space. The errosol can is free to return to the rest position under the action of its own serosol valve spring.

In use the patient loads the serosol dispensing container into the main body, which comprises upper and lower sections of joined by a threaded connector part 505. When the sections of the main body 400 are separated, the aerosol can be inserted. The main body 400 can them be replaced locating the inner alsewe over the top end of the can, and the device is ready for use. As described previously, the device could be nummfactured as a sealed unit.

The device may be provided with means to provide a regulated air flow to the user or inhaler. Thus a sonic device, e.g., a read, may be provided which sounds when the inspired air flow is greater than a pre-set level, e.g., above to 50 litres per simits. The sonic device may be located in the nouthplace 95 or below the air inlet 420. The sound produced warms the patient to breathe at a lower rate.

The device may also be provided with a means such that it vill not operate below a certain predetermined oir flow rate, e.g., 10 to 10 litres per minute. In one embodisent the vance 550 or 110 will be biased by a spring such that the predetermined minium air flow is necessary for it to sowe to its actuated position and enable the valve seal to open.

The main body of a dispensing device, as described in this embodiment of this invention is preferably memfactured from a plastics material such as polypropylane, acetal or moulded polystyrene. It say however he manufactured from matal or another suitable material. occurs before the aerosol valve has been sufficiently compressed to actuate it.

A typical aerosol requires about 200 force to actuate. The spring 460 should accordingly provide a greater force; preferably 10% to 50% greater.

It may also be possible to arrange for the balance of forces to take place before the inner sleeve has contacted the aerosol can, such that the spring force is balanced by the resisting force produced on the inner sleeve by virtue of the pressure differential.

on inhalation by the patient through the nouthpiece 405, a small pressure differential is created across the wane 550 which is pluvted towards one end. The pressure differential causes the wans to move from the rest position to its actual position. The wans and design of the air passegoway 500 in the chamber 590 are such that in the actuated position air can flow freely from the air inlets 420 to the patient.

The novement of the vens 550 causes the valve seal element 340 to be noved out of a sealing position with the valve port 495 as shown in Fig. 2. Opening the valve port allows air into the gap 600 between the disphrays and inner slower such that the enclosed space reaches etmospheric pressure. This causes an inhalance of forces acting on the sleeve 420 and container 25. The sleeve and cuntainer are thus forced downwards by the spring 460 resulting in the release of a measured dose of medicament through the dispensing nossie 55 and into the mouthplace at the same time as the patient breaths in. Thus the patient inhales air with a metered dose of medicament.

After the inhelation of the dose by the patient, the dust cap 510 is returned to its closed position. This rotates the cas 520 and causes the cas follows 530 to be forced upwards. This in turn acts on the inner sleeve 420 moving it upwards to compress the spring 450 and close the gap 600 between the disphragm and inner sleeve top surface 422. This forces air out of the enclosed space 600 which escapes through the valve port 435 lifting the valve seal element 540. Since the valve

- 12 -

## CLAIKS

- A dispensing device for use with a drug delivery system, the dispensing device comprising means for releasing a dose of pedicament from the system, the releasing means comprising means for applying a preload capable of actuating the drug delivery system to dispense a dose of medicament, s for applying a resisting pneumatic or other gas force capable of preventing actuation of the drug delivery system, and a release device capable of freeing the resisting pneumatic force to allow the preload to actuate the delivery means and dispense the medicament, wherein said resisting matic force is provided by a volume of gas held at a positive or negative pressure with respect to ambient pressure, and said release means comprise a flexible plate-like sealing element which seals with a valve seat nd a valve port, the opening of which releases said positive or negative pressure, the sealing element being carried by a sealing member such that, on initial novement of the sealing member, the scaling element flexes as it is hald by said positive or negative pressure against the valve soat until it is finally removed therefrom on further powement of the sealing ment
- A dispensing device according to Claim 1, wherein said release device is edapted to remove said scaling element from said valve seat in response to inhalation at an owtlet notate of the device.
- 3. A dispensing device according to Claim 2, wherein said sealing member comprises a novable vane, which on imbalation is capable of noving from a rest position to an actuating position theraby removing said disphraga sealing almost from said valve seat.
- 4. A dispensing device according to Claim 3, wherein said wans constitutes one section of a pivotal mounted lever, said diaphraga sealing element being carried by a second

section of the lever on the opposite side of the pivot to said

- 5. A dispensing device according to any preceding claim, wherein caid sealing element is a flexible disphreya sealing element held at its periphary by said sealing member to provide a freely floxible central part which cooperates with said valve seat.
- 6. A dispensing device according to any preceding claim, further including a housing providing a chamber for receiving said drug delivery system in the form of an acrosol container, with an inner sleave being elidably mounted within the chamber for at least partly enclosing the main body of an acrosol container, when disposed, in use, in said chamber.
- 7. A dispensing device according to Claim 6, wherein said resisting pnematic pressure is a positive pressure created by cooperation between said inner sleave and a cross neaber provided in the housing, to form a piston and cylinder assembly.
- a dispensing device according to Claim 7, wherein said valve port is provided in said cross member.
- 9. A dispensing device as claimed in any one of Claims 1 - 6, wherein esid passmatic resisting force is a negative pressure created inside an expandable airtight volume defined by a ballows, piston, cylinder or diaphrage.
- 10. A dispensing device as claimed in Claims 6 and 9, wherein said sirtight volume is defined between a disphragm which is scaled with respect to a closed end of said inner sleeve, with said valve port being provided in said disphragm.
- A dispensing device according to any one of Claims 6 - 0 and 10, wherein said actuating means act on said

- 15-Application number Patents Act 1977 Examiner's report to the Comptroller under Section 17 (The Search Report) 9211434.7 Search Examiner Relevant Technical fields (i) UK CI (Edition K ) AST TRO, TRE J A BALLIS (ii) Int CI (Edition 5 ) ASIM Date of Search Databasas (see over) (i) UK Patent Office 19 ADGUST 1992 OFFLIRE DATABASES: WPI Documents considered relevant following a search in respect of claims

1 AT LEAST

Catagory (see over)	kiemity of document and relevant pessages	Relevent to claim(s)
	FUEL	
F2(p)	17 - docs5\fi	1000258

inner sleaver, and wherein means are provided for resetting said actuating means after release thereof to cause actuation of the drug delivery system.

- 12. A dispensing device as claimed in Claim 11, having a housing provided with an outlet nossle and a cover for the nossle novably mounted on said housing, wherein a control member associated with said inner sleeve cooperates with a cas formation provided on the cover such that, when the cover is closed, the control member noves the inner sleeve to reset said actuating means and, when the cover is opened, the inner sleeve is goved under the action of the spring until the forces acting on the inner sleeve, including said posumatic resisting force are balanced, preparatory to release of the posumatic resisting force in response to inhalation at said nossile.
- 13. A dispensing device according to any preceding claim, wherein said actuating means comprise resilient means for actuating the drug delivery system on release of said valence means.
- 14. A dispensing device substantially as hereinbefore described with reference to the accompanying drawings.
- 15. A dispensing device according to any one of the preceding claims in combination with a drug delivery system in the form of an aerosol dispensing container having a valve capable of being actuated to release a netered amount of the pressurized aerosol contents.
- 16. A dispensing drvice according to any one of Claims 1 - 5, 9 - 13 in combination with a dry powder drug delivery system which is adapted to dispense, when actuated, a does of newdered redispense.

-16 -				
Category	Identity of document and relave	et passages	Referent to claim(s)	
		<del></del>		
-				
}				
1				
1				
			ł	
1			Í	
1				
i				
- 1			i	
			ŀ	
1				
			1	
			İ	
			1	
Categories of			• • • •	
X: Document indicating fact of navelty or of inventive step.		P. Document published on or after the declared priority data but before the filing data of the present application.		
Y: Document indicating back of inventive stop if countries with one or more other documents of the same category.		E: Patiest document published on or after, but with priority date earlier than, the filing date of the present application.		
At Document Indicating technological background earlier state of the ST.		& Mander of the same parent family.		

Databasses: The UX Peters Office database comprises described collections of Gb, EP, WO and US peters specifications as outlined perfodicibly in the Official Journal Phenrick. The ordine databases considered to search are sim bent perfodicibly in the Official Journal (Peters).